International Tables for Crystallography (2018). Vol. H, Section 2.1.7.1, pp. 45–46.

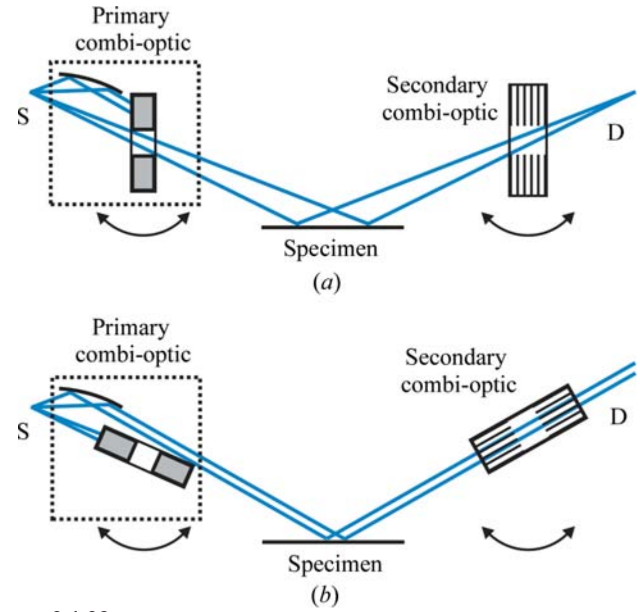

Figure 2.1.23
Incident and diffracted beam combi-optics for switching between (*a*) the Bragg–Brentano geometry and (*b*) the parallel-beam geometry. S: X-ray source; D: detector.

separated by a small gap. When turning the two parallel-plate collimators into the beam direction, only those diffracted rays running parallel to the collimator plates will reach the detector (Fig. 2.1.23*b*). When turning the collimators by approximately 90°, the gap between the two collimators acts as a variable slit enabling a divergent beam (Fig. 2.1.23*a*).

Significantly more sophisticated combi-optics are used in X-ray diffractometers that are mostly used for thin-film analysis. In Fig. 2.1.24 an example for two different incident-beam and four different diffracted-beam paths is shown, providing the choice between eight different beam paths depending on the properties of the specimen and the application requirements. The incident beam path is characterized by a fixed-target X-ray source equipped with a Göbel mirror, attached on a motorized mount. By rotating this arrangement by about 5°, the beam travels either through a rotary absorber followed by a two-bounce channel-cut monochromator and a slit (upper beam path, high-resolution setting), or just through a single slit (lower beam path, high-flux setting). The diffracted beam path represents a double-detector setup, typically consisting of a point detector (D1) and a position-sensitive detector (D2). For the point detector three different beam paths can be chosen by means of a switchable slit, which either sends the beam through a three-bounce channel-cut analyser, or through the same two-parallel-plate-collimator arrangement already discussed in Fig. 2.1.23, either acting as a parallel-plate collimator or a variable slit. A fourth beam path without any diffracted-beam X-ray optics allows use of the position-sensitive detector.

2.1.7. X-ray detectors

The general concepts of X-ray detectors are described here with the focus on practical aspects. The physics of X-ray detection and the individual detector technologies are extensively covered in the literature. He (2009) gives a comprehensive discussion that also includes the most recent detector technologies. Additional detailed descriptions are found in *International Tables for Crystallography* Vol. C (2004), as well as in the textbooks by Pecharsky & Zavalij (2009), Clearfield *et al.* (2008), Paganin (2006), Jenkins & Snyder (1996), and Klug & Alexander (1974).

2.1.7.1. *Detector parameters*

There are many ways to characterize the properties and performance of an X-ray detector.

Ideally, in a given detector operated under appropriate conditions, (1) each photon will produce a detectable signal and (2) the signal recorded is proportional to the number of photons detected. If both conditions are fulfilled then the detector has unit *quantum efficiency*. The *detective quantum efficiency* (DQE) may be defined as the squared ratio of the output signal-to-noise ratio to the input signal-to-noise ratio, expressed as a percentage. A detector's DQE is generally less than 100% because there is always detector noise and not every photon is detected. The DQE thus depends on the characteristics of the detector (*e.g.* transmission of the detector window, count rates and dead time, *etc.*) and varies with the X-ray energy for the same detector.

The *detector linearity* determines the accuracy of intensity measurements and depends on the ratio between the photon

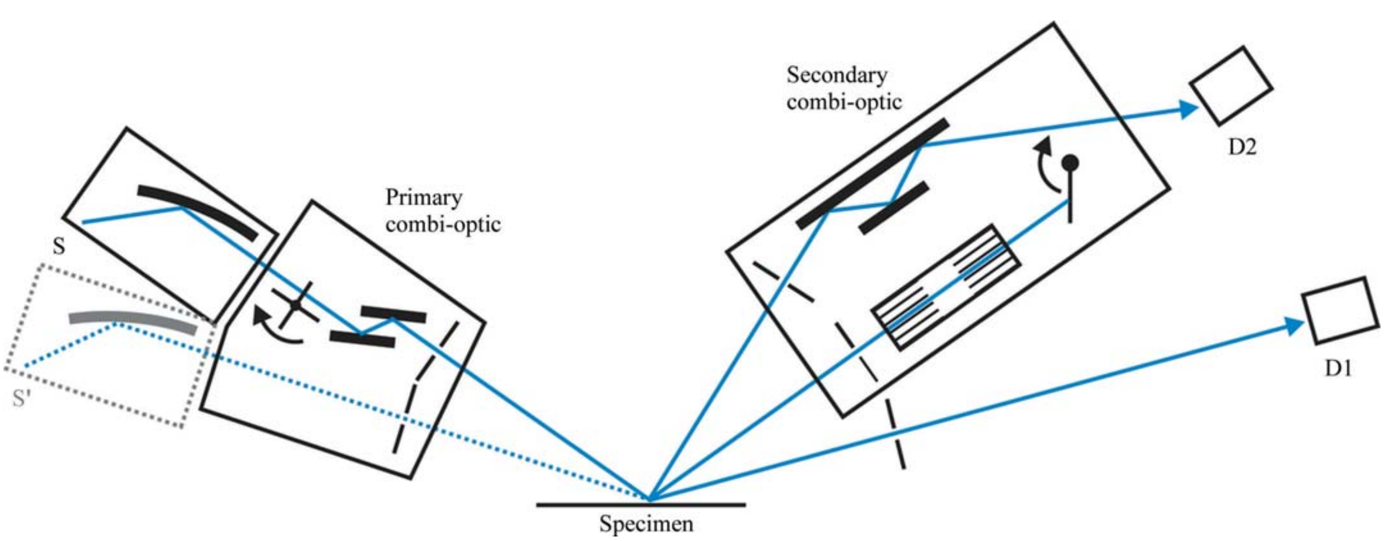

Figure 2.1.24
Example of the use of highly sophisticated incident- and diffracted-beam combi-optics in combination with a rotatable X-ray source and a double detector arm. This setup enables two different incident-beam and four different diffracted-beam paths, and thus provides a choice between eight different beam paths, depending on the properties of the specimen and the requirements of the application. S: X-ray source, S′: X-ray source rotated by about 5°, D1, D2: detectors.

count rate and the rate of signals generated and registered by the detector. In any detector it takes some time to process the conversion of an individual photon to a voltage pulse, which is related to the detector *dead time*: photons arriving while the detector is still processing the previous photon conversion may be lost. The detector dead time is related to the physical characteristics of the detector, *e.g.* the drift time in a gas-ionization detector, or the read-out time of the counting electronics, *e.g.* the shaping time of the amplifier. The effect of dead time becomes a substantial issue at high photon count rates, when the dead time becomes a significant part of the average time separation between two arriving photons, leading to increasing intensity losses at higher count rates. Detectors can be categorized as being non-paralysable or paralysable with respect to dead time. A non-paralysable detector is dead for a fixed time after each count, but not influenced by photons arriving during the dead time. Counting losses increase with increasing count rates, but the true count rate of a nonparalysable detector can be corrected unless the maximum observed count rate is equal to the inverse of the dead time. In a paralysable detector, a second photon arriving within the dead time can not be counted but will extend the dead time up to a point where the detector will be incapable of collecting any counts at all (saturation point). Modern detectors can stand the count rates obtained in powder diffraction experiments using fixed-target X-ray sources. At very high count rates, *e.g.* those obtained in thin-film experiments such as reflectometry, it may be necessary to attenuate the beam. Sophisticated instruments are equipped with an electronic feedback system and automatic absorbers (see Section 2.1.6.3.1.2) to ensure that detector saturation is avoided.

The *dynamic range* of a detector may be defined as the range between the smallest detectable photon count rates (determined by inherent detector noise such as readout and dark noise) to the largest acceptable photon count rates (determined by the dead time).

Energy resolution is the ability of a detector to resolve two photons that have different energies. Energy resolution is typically characterized by the size of the detector energy window, ΔE, in electron volts, as determined by the full width at half maximum (FWHM) of the detector-efficiency curve as a function of energy, with the detector and counting electronics set to a specific wavelength. Another frequently used expression for energy resolution is the ratio of the detector energy window size to the energy of the monochromatic X-ray beam, E, expressed as $\Delta E/E$.

The *proportionality* of the detector determines how the size of the generated voltage pulse is related to the energy of the absorbed X-ray photons, and electronic methods (pulse-height selection) can be used to discriminate between different energies. An accurate proportionality thus allows the use of *energy discrimination* as a form of monochromatization, where the energy is filtered by the detector rather than by an optical element such as a metal filter, crystal or mirror; see Section 2.1.6.3. Signals corresponding to photons with too high or too low energies are discarded.

The size and weight of detectors may impose several practical constraints, see also Section 2.1.4.2. For large detectors the accessible angular range may be limited owing to collision issues. For heavy detectors a horizontal goniometer may be preferred over a vertical goniometer (unless horizontal specimen positioning is imperative) in order to minimize the goniometer load.

X-ray detectors may be broadly classified as *counting detectors* or *integrating detectors*. Counting (digital) detectors are able to detect and count individual photons. The number of pulses counted per unit time is proportional to the incident X-ray flux. Integrating (or analogue) detectors accumulate photon-induced signals for a given period of time, prior to the integrated signal being read out and converted into an (analogue) electrical signal. The signal size is proportional to the flux density of the incident X-rays.

Counting and integrating detectors each have their clear advantages and disadvantages. Counting detectors normally have a greater dynamic range than integrating detectors, while integrating detectors normally have better spatial resolution (Section 2.1.7.3). Energy resolution is only possible for counting detectors. Readout and dark noise are usually higher for integrating detectors. Integrating detectors are not limited by the photon count rate as there is no dead time; nevertheless, the measurement time has to be kept sufficiently small to avoid saturation.

2.1.7.2. *Detector types*

Counting and integrating detectors can be further distinguished by their working principle, and are represented by scintillation, gas-ionization and semiconductor detectors. The most commonly used detector types and their properties are listed in Tables 2.1.1 and 2.1.6, respectively.

At the end of the 1990s the types of detectors in use were scintillation, gas-ionization, Si(Li) and image-plate detectors, with the scintillation counter being the most common by far. Usage of photographic film had already greatly diminished by that time. With the introduction of a series of new one- and two-dimensional detector technologies since the late 1990s, the X-ray detection landscape changed completely. New semiconductor-based detectors (silicon micro-strip, silicon pixel) as well as gas-ionization-based detectors (micro-gap) reached a market share of >90% in newly sold X-ray powder diffractometers within only a few years. As a consequence, classical metal-wire-based proportional counters and scintillation counters will probably become obsolete before 2020. The same is expected for CCD-based detectors, which will be replaced by the very recently introduced complementary metal–oxide–semiconductor (CMOS) active pixel sensor technology.

In the following the working principles of currently available detector types will be briefly described. Matters that are specific to zero- (0D), one- (1D) and two-dimensional (2D) detection are discussed in Section 2.1.7.3. While image plates are still in use, their market share in newly sold systems has become insignificant. Photographic film techniques are totally obsolete. For these reasons, these two detector types will not be taken into further consideration.

2.1.7.2.1. *Scintillation counters*

Scintillation counters are constructed from a scintillator crystal optically coupled to a photomultiplier tube. The crystal is typically made of sodium iodide (NaI) doped with about 1% thallium, frequently denoted as NaI(Tl). When irradiated by X-ray radiation, blue light (~415 nm) is emitted and converted to electrons in a photomultiplier and amplified; the resulting pulses are registered as photon counts.

The height of the outgoing pulses is proportional to the energy of the incoming X-ray photons. This permits the use of pulse-height selection but only allows for poor energy resolution. The relatively high count rate and a moderate noise level result in a moderate dynamic range. These characteristics are the reason for the formerly wide-ranging acceptance of the scintillation counter